

# Infection Control and Hospital Epidemiology

## Addressing Personal Protective Equipment (PPE) Decontamination: Methylene Blue and Light Inactivates SARS-CoV-2 on N95 Respirators and Medical Masks with Maintenance of Integrity and Fit

--Manuscript Draft--

<b>Manuscript Number:</b>	
<b>Full Title:</b>	Addressing Personal Protective Equipment (PPE) Decontamination: Methylene Blue and Light Inactivates SARS-CoV-2 on N95 Respirators and Medical Masks with Maintenance of Integrity and Fit
<b>Short Title:</b>	Using methylene blue and light to decontaminate PPE for reuse and wear
<b>Article Type:</b>	Original Article
<b>Corresponding Author:</b>	Thomas Sean Lendvay, M.D. University of Washington School of Medicine, Seattle Children's Hospital Seattle, WA UNITED STATES
<b>Corresponding Author Secondary Information:</b>	
<b>Corresponding Author's Institution:</b>	University of Washington School of Medicine, Seattle Children's Hospital
<b>Corresponding Author's Secondary Institution:</b>	
<b>First Author:</b>	Thomas Sean Lendvay, M.D.
<b>First Author Secondary Information:</b>	
<b>Order of Authors:</b>	Thomas Sean Lendvay, M.D. James Chen Brian H Harcourt, PhD Florine EM Scholte, PhD Ying Ling Lin, PhD F Selcen Kilinc-Balci, PhD Molly M Lamb, PhD Kamonthip Homdayjanakul, MPH Yi Cui, PhD Amy Price, MS, MA, DrPhil Belinda Heyne, PhD Jaya Sahni, PhD Kareem B Kabra, MS Yi-Chan Lin, PhD David Evans, PhD, BSc Chris N Mores, SM, ScD Ken Page, BA Larry F Chu, MS, MD Eric Haubruge, Prof ., PhD, M.S.Eng ., B.S.Eng ., D.h.c. Etienne Thiry, Prof ., D . V . M ., PhD Louisa F Ludwig-Begall, DVM

Constance Wielick, DVM
Tanner Clark, MD
Thor Wagner, MD
Emily Timm, PhD
Thomas Gallagher, PhD
Peter Faris
Nicolas Macia, PhD
Cyrus J Mackie
Sarah M Simmons, PhD
Susan Reader, BN, MAL
Rebecca Malott, PhD
Karen Hope, MSc
Jan M Davies, FRCPC
Sarah R Tritsch, MS
Lorène Dams, BSc
Hans Nauwynck, Prof ., D . V . M ., PhD
Jean-Francois Willaert, M.S.Eng ., B.S.Eng .
Simon De Jaeger, MSc
Lei Liao, PhD
Mervin Zhao, PhD
Jan Laperre, PhD
Oliver Jolois
Sarah J Smit
Alpa N Patel, BS
Mark Mayo, HND
Rod Parker, PhD
Vanessa Molloy-Simard, M.Sc., Mcb.A., RMCCM
Jean-Luc Lemyre, PhD
Steven Chu, PhD
John M Conly, MD
May C Chu, PhD

**Order of Authors Secondary Information:**

**Abstract:**

Objective: The coronavirus disease 2019 (COVID-19) pandemic has resulted in shortages of personal protective equipment (PPE) underscoring the urgent need for simple, efficient, and inexpensive methods to decontaminate SARS-CoV-2-exposed masks and respirators. We hypothesized that methylene blue (MB) photochemical treatment, which has various clinical applications, could decontaminate PPE contaminated with coronavirus.

Design: The two arms of the study included: 1) PPE inoculation with coronaviruses followed by MB with light (MBL) decontamination treatment, and 2) PPE treatment with MBL for 5 cycles of decontamination (5CD) to determine maintenance of PPE performance.

Methods: MBL treatment was used to inactivate coronaviruses on three N95 filtering facepiece respirator and two medical mask models. We inoculated FFR and MM

materials with three coronaviruses, including SARS-CoV-2, and treated with 10  $\mu$ M MBL and exposed to 50,000 lux of white light or 12,500 lux of red light for 30 minutes. In parallel, integrity was assessed after 5CD using multiple US and international test methods and compared to the FDA-authorized vaporized hydrogen peroxide plus ozone (VHP+O<sub>3</sub>) decontamination method.

Results: Overall, MBL robustly and consistently inactivated all three coronaviruses with 99.8 - to >99.9% virus inactivation across all FFRs and MMs tested. FFR and MM integrity was maintained after 5 cycles of MBL treatment, whereas one FFR model failed after 5 cycles of VHP+O<sub>3</sub>.

Conclusions: MBL treatment decontaminated respirators and masks by inactivating three tested coronaviruses without compromising integrity through 5CD. MBL decontamination is effective, low-cost and does not require specialized equipment, making it applicable in all-resource settings.

Dear Editors of Infection Control and Hospital Epidemiology,

We cannot continue to be oppressed by the COVID19 pandemic.

Whether it be from global underestimation of the far-reaching impact of a pandemic or whether due to political ambivalence, our healthcare workers and global citizens do not have the adequate supply of personal protective equipment needed to mitigate the spread of SARS-CoV-2. This supply shortage requires a decontamination solution that is simple, safe, inexpensive, resource-light and globally accessible. In our study, the first of its kind, we have shown that methylene blue (MB, a common dye) when activated with bright white light, can inactivate human SARS-CoV-2 on commonly used N95 respirators, medical masks, and community masks without degrading the PPE materials.

We represent a consortium of virology labs and mask and respirator integrity testing sites around the globe (including the National Institute of Occupational Safety and Health) testing the hypotheses that methylene blue with light can inactivate coronaviruses on PPE. Our team is comprised of members of the WHO Infection Prevention and Control (IPC) Group, the WHO COVID 19 Task Force, and the Centers for Disease Control and Prevention in the US. Three different coronaviruses were tested – Human SARS-Co-V-2, Murine Hepatitis Virus (MHV), and a porcine coronavirus to understand the inactivation potential of methylene blue.

We leveraged existing clinical evidence of the safety and efficacy of methylene blue and its ability to generate singlet oxygen to develop a potential recipe for PPE decontamination. Furthermore, we are adding to the literature about the stable integrity of PPE when subjected to repeated (X5) cycles of MB decontamination. These data provide guidance and reassurance to the PPE wearer that reuse of PPE is not providing additional risk in high exposure environments and situations.

In the course of this study, one of our senior researchers lost her husband to COVID19 making the need to get our results and message to the globe that more pressing.

All authors have approved this manuscript, contributed significantly to this work, and this manuscript has not been previously published in a peer reviewed journal, nor is being considered by another journal for publication. We have pre-published the methylene blue details in MedRxiv doi: <https://doi.org/10.1101/2020.12.11.20236919>

We suggest the following four thought leaders as potential reviewers for this manuscript:

- 1) Scott C. Weaver, MS, PhD, Galveston National Laboratory, [sweaver@utmb.edu](mailto:sweaver@utmb.edu)
- 2) Trish M Perl, MD, MSc, UT-Southwestern, [trish.perl@UTSouthwestern.edu](mailto:trish.perl@UTSouthwestern.edu)
- 3) Daniel G. Bausch, MD, MPH, TM, Public Health England/London School of Hygiene and Tropical Medicine, [Daniel.Bausch@phe.gov.uk](mailto:Daniel.Bausch@phe.gov.uk)
- 4) Armand Sprecher, MD, MPH, Médecins Sans Frontières, Operational Center Brussels, [armand.sprecher@brussels.msf.org](mailto:armand.sprecher@brussels.msf.org)

We thank you for the opportunity to submit this research to a wide and diverse community.

Sincerely,

Thomas Lendvay, MD FACS and May Chu, PhD

Thomas Lendvay, MD FACS  
Professor, Department of Urology  
University of Washington  
Seattle Children's Hospital  
4800 Sand Point Way NE  
Seattle, Washington, 98105  
USA  
Cell# +1-206-349-2212  
Fax# +1-206-987-3925  
Email: [thomas.lendvay@seattlechildrens.org](mailto:thomas.lendvay@seattlechildrens.org)  
First and Corresponding Author

May Chu, PhD  
Professor, Center for Global Health  
Colorado School of Public Health, Anschutz Medical Campus  
Aurora, Colorado, 80045  
USA  
Cell#+1-770-688-5006  
Email: [may.chu@cuanschutz.edu](mailto:may.chu@cuanschutz.edu)  
Senior Author

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

1

# Addressing Personal Protective Equipment (PPE)

1

## Decontamination: Methylene Blue and Light Inactivates

2

## SARS-CoV-2 on N95 Respirators and Medical Masks

3

### with Maintenance of Integrity and Fit

4

5 Thomas Sean Lendvay, MD, Department of Urology, University of Washington School of  
6 Medicine, Seattle Children's Hospital, Seattle, Washington, USA

7

8 James Chen, MD, Department of Urology, University of Washington School of Medicine,  
9 Seattle Children's Hospital, Seattle, Washington, USA

10

11 Brian H Harcourt, PhD, Viral Special Pathogens Branch, Division of High Consequence  
12 Pathogens and Pathology, National Center for Emerging and Zoonotic Infectious Diseases,  
13 Centers for Disease Control and Prevention, Atlanta, Georgia, USA

14

15 Florine EM Scholte, PhD, Department of Infectious Diseases, Microbiology and Immunology,  
16 CRCHU de Québec-Université Laval, Québec, QC, Canada Atlanta, Georgia, USA

17

18 Ying Ling Lin, PhD, World Health Organization, Geneva, Switzerland

19

1  
2  
3 20 F Selcen Kilinc-Balci, PhD, National Personal Protective Technology Laboratory (NPPTL),  
4  
5  
6 21 National Institute for Occupational Safety and Health, Centers for Disease Control and  
7  
8 22 Prevention, Pittsburgh, Pennsylvania, USA  
9  
10 23  
11  
12  
13 24 Molly M Lamb, PhD, Center for Global Health, Colorado School of Public Health, Anschutz  
14  
15 25 Medical Campus, Aurora, Colorado, USA  
16  
17  
18 26  
19  
20 27 Kamonthip Homdayjanakul, MPH, Center for Global Health, Colorado School of Public Health,  
21  
22  
23 28 Anschutz Medical Campus, Aurora, Colorado, USA  
24  
25 29  
26  
27 30 Yi Cui, PhD, Department of Materials Science and Engineering, Stanford University, Stanford,  
28  
29 31 California, USA  
30  
31  
32 32  
33  
34  
35 33 Amy Price, MA, MS, DrPhil, The AIM Lab, Stanford University School of Medicine, Stanford,  
36  
37 34 California USA.  
38  
39  
40 35  
41  
42 36 Belinda Heyne, PhD, Department of Chemistry, University of Calgary, Calgary, Alberta, Canada  
43  
44 37  
45  
46  
47 38 Jaya Sahni, PhD, Seattle Children's Research Institute, Seattle, Washington USA  
48  
49 39  
50  
51  
52 40 Kareem B Kabra, MS, Department of Global Health, Milken Institute School of Public Health,  
53  
54 41 The George Washington University, Washington, DC, USA  
55  
56  
57 42  
58  
59  
60  
61  
62  
63  
64  
65

1  
2  
3 43 Yi-Chan Lin, PhD, Department of Medical Microbiology and Immunology, University of  
4  
5  
6 44 Alberta, Edmonton, Alberta, Canada.  
7  
8 45  
9  
10 46 David Evans, PhD, BSc, Department of Medical Microbiology and Immunology, University of  
11  
12 47 Alberta, Edmonton, Alberta, Canada.  
13  
14  
15 48  
16  
17 49 Christopher N Mores, SM ScD, Department of Global Health, Milken Institute School of Public  
18  
19 50 Health, The George Washington University, Washington, DC, USA  
20  
21  
22 51  
23  
24 52 Ken Page, BA, Alberta Health Services, Alberta, Canada.  
25  
26  
27 53  
28  
29 54 Larry F Chu, MS, MD, The AIM Lab, Stanford University School of Medicine, Stanford,  
30  
31 55 California USA.  
32  
33  
34 56  
35  
36 57 Eric Haubruge, Prof ., PhD, M.S.Eng ., B.S.Eng ., D.h.c., Gembloux AgroBioTech, Terra  
37  
38 58 Research Center, University of Liège, Gembloux, Belgium.  
39  
40  
41 59  
42  
43 60 Etienne Thiry, Prof ., D . V . M ., PhD, Department of Infectious and Parasitic Diseases, Faculty  
44  
45 61 of Veterinary Medicine, University of Liège, Liège, Belgium  
46  
47  
48 62  
49  
50 63 Louisa F Ludwig-Begall, D . V . M ., Department of Infectious and Parasitic Diseases, Faculty of  
51  
52 64 Veterinary Medicine, University of Liège, Liège, Belgium  
53  
54  
55 65  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65



1  
2  
3 66 Constance Wielick, D . V . M., Department of Infectious and Parasitic Diseases, Faculty of  
4  
5  
6 67 Veterinary Medicine, University of Liège, Liège, Belgium  
7  
8 68  
9  
10  
11 69 Tanner Clark, MD, Department of Radiology, University of Washington School of Medicine,  
12  
13 70 Seattle, Washington, USA  
14  
15 71  
16  
17  
18 72 Thor Wagner, MD, Seattle Children’s Research Institute, Seattle, Washington USA  
19  
20 73  
21  
22  
23 74 Emily Timm, PhD, Department of Microbiology and Immunology, Loyola University Chicago,  
24  
25 75 Maywood, Illinois, USA.  
26  
27 76  
28  
29  
30 77 Thomas Gallagher, PhD, Department of Microbiology and Immunology, Loyola University  
31  
32 78 Chicago, Maywood, Illinois, USA.  
33  
34  
35 79  
36  
37 80 Peter Faris, Alberta Health Services, Alberta, Canada.  
38  
39  
40 81  
41  
42 82 Nicolas Macia, PhD, Department of Chemistry, University of Calgary, Calgary, Alberta, Canada  
43  
44 83  
45  
46  
47 84 Cyrus J Mackie, Department of Chemistry, University of Calgary, Calgary, Alberta, Canada  
48  
49 85  
50  
51  
52 86 Sarah M Simmons, PhD, W21C Research and Innovation Centre, University of Calgary,  
53  
54 87 Calgary, Alberta, Canada  
55  
56  
57 88  
58  
59 89 Susan Reader, BN, MAL, Alberta Health Services, Alberta, Canada.  
60  
61  
62  
63  
64  
65

1  
2  
3  
4 90  
5  
6 91 Rebecca Malott, PhD, W21C Research and Innovation Centre, University of Calgary, Calgary,  
7  
8 92 Alberta, Canada  
9  
10 93  
11  
12  
13 94 Karen Hope, MSc, Alberta Health Services, Alberta, Canada.  
14  
15 95  
16  
17  
18 96 Jan M Davies, FRCPC, W21C Research and Innovation Centre, University of Calgary, Calgary,  
19  
20 97 Alberta, Canada Alberta Health Services, Alberta, Canada, Department of Anesthesiology,  
21  
22 98 Perioperative and Pain Medicine, University of Calgary, Calgary, Alberta, Canada  
23  
24  
25 99  
26  
27  
28 100 Sarah R Tritsch, MS, Department of Global Health, Milken Institute School of Public Health,  
29  
30 101 The George Washington University, Washington, DC, USA  
31  
32  
33 102  
34  
35 103 Lorène Dams, B.S c., Department of Infectious and Parasitic Diseases, Faculty of Veterinary  
36  
37 104 Medicine, University of Liège, Liège, Belgium  
38  
39  
40 105  
41  
42 106 Hans Nauwynck, Prof ., D . V . M ., PhD, Faculty of Veterinary Medicine, Ghent University,  
43  
44 107 Merelbeke, Belgium.  
45  
46  
47 108  
48  
49  
50 109 Jean-Francois Willaert, M.S.Eng ., B.S.Eng, Gembloux AgroBioTech, Terra Research Center,  
51  
52 110 University of Liège, Gembloux, Belgium.  
53  
54  
55 111  
56  
57 112 Simon De Jaeger, M.S c, Department of Infectious and Parasitic Diseases, Faculty of Veterinary  
58  
59 113 Medicine, University of Liège, Liège, Belgium  
60  
61  
62  
63  
64  
65

1  
2  
3 114  
4  
5  
6 115 Lei Liao, PhD, 4CAir, Inc., Sunnyvale, California, USA  
7  
8 116  
9  
10  
11 117 Mervin Zhao, PhD, 4CAir, Inc., Sunnyvale, California, USA  
12  
13 118  
14  
15 119 Jan Laperre, PhD, Centexbel, Grace-Hollogne, Belgium  
16  
17  
18 120  
19  
20 121 Olivier Jolois, Centexbel, Grace-Hollogne, Belgium  
21  
22  
23 122  
24  
25 123 Sarah J Smit, Nelson Laboratories, LLC, Salt Lake City, Utah, USA  
26  
27  
28 124  
29  
30 125 Alpa N Patel, BS, Nelson Laboratories, LLC, Salt Lake City, Utah, USA  
31  
32  
33 126  
34  
35 127 Mark Mayo, HND, British Standards Institution, London, United Kingdom.  
36  
37  
38 128  
39  
40 129 Rod Parker, PhD, Stryker, Quebec, Canada.  
41  
42  
43 130  
44  
45 131 Vanessa Molloy-Simard, M.Sc., Mcb.A., RMCCM, Stryker, Quebec, Canada.  
46  
47  
48 132  
49  
50 133 Jean-Luc Lemyre, PhD, Stryker, Quebec, Canada.  
51  
52  
53 134  
54  
55 135 Steven Chu, PhD, Department of Physics, Molecular and Cellular Physiology, Stanford  
56  
57 136 University, Stanford, California, USA.  
58  
59  
60 137  
61  
62  
63  
64  
65

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

138 John M Conly, MD, W21C Research and Innovation Centre, University of Calgary, Calgary,  
139 Alberta, Canada Alberta Health Services, Alberta, Canada

140  
141 May C Chu, PhD, Center for Global Health, Colorado School of Public Health, Anschutz  
142 Medical Campus, Aurora, Colorado, USA

144 **Keywords:**

145 methylene blue, PPE decontamination, SARS-CoV-2, respirators, fit, COVID-19,  
146 photochemistry

147 **Running title:**

148 Using MB to decontaminate PPE for reuse and wear

149 **Correspondence to:**

150 Thomas S. Lendvay, MD

151 Professor, Department of Urology, University of Washington

152 Seattle Children’s Hospital

153 Address: 4800 Sand Point Way NE, Seattle, WA, 98105

154 Email: [thomas.lendvay@seattlechildrens.org](mailto:thomas.lendvay@seattlechildrens.org)

155 Cell phone: (+1)206-349-2212

156 Office phone: (+1)206-987-4403

157 **Word count:** 2,984 – Introduction, Methods, Results, Discussion

158

159

1  
2  
3 160 **ABSTRACT**

4  
5  
6 161 **Objective:** The coronavirus disease 2019 (COVID-19) pandemic has resulted in shortages of  
7  
8  
9 162 personal protective equipment (PPE) underscoring the urgent need for simple, efficient, and  
10  
11 163 inexpensive methods to decontaminate SARS-CoV-2-exposed masks and respirators. We  
12  
13 164 hypothesized that methylene blue (MB) photochemical treatment, which has various clinical  
14  
15 165 applications, could decontaminate PPE contaminated with coronavirus.

16  
17  
18 166 **Design:** The two arms of the study included: 1) PPE inoculation with coronaviruses followed by  
19  
20 167 MB with light (MBL) decontamination treatment, and 2) PPE treatment with MBL for 5 cycles  
21  
22  
23 168 of decontamination (5CD) to determine maintenance of PPE performance.

24  
25 169 **Methods:** MBL treatment was used to inactivate coronaviruses on three N95 filtering facepiece  
26  
27 170 respirator and two medical mask models. We inoculated FFR and MM materials with three  
28  
29  
30 171 coronaviruses, including SARS-CoV-2, and treated with 10 µM MB and exposed to 50,000 lux  
31  
32 172 of white light or 12,500 lux of red light for 30 minutes. In parallel, integrity was assessed after  
33  
34  
35 173 5CD using multiple US and international test methods and compared to the FDA-authorized  
36  
37 174 vaporized hydrogen peroxide plus ozone (VHP+O<sub>3</sub>) decontamination method.

38  
39  
40 175 **Results:** Overall, MBL robustly and consistently inactivated all three coronaviruses with 99.8 -  
41  
42 176 to >99.9% virus inactivation across all FFRs and MMs tested. FFR and MM integrity was  
43  
44  
45 177 maintained after 5 cycles of MBL treatment, whereas one FFR model failed after 5 cycles of  
46  
47 178 VHP+O<sub>3</sub>.

48  
49  
50 179 **Conclusions:** MBL treatment decontaminated respirators and masks by inactivating three tested  
51  
52 180 coronaviruses without compromising integrity through 5CD. MBL decontamination is effective,  
53  
54  
55 181 low-cost and does not require specialized equipment, making it applicable in all-resource  
56  
57 182 settings.

58  
59 183  
60  
61  
62  
63  
64  
65

1  
2  
3  
4 184 **INTRODUCTION**

5  
6 185 The coronavirus disease 2019 (COVID-19) pandemic caused by SARS-CoV-2 has  
7  
8 186 resulted in critical personal protective equipment (PPE) shortages, especially filtering facepiece  
9  
10 187 respirators (FFRs, also known as N95 respirators). Although designed for single use, healthcare  
11  
12  
13 188 personnel (HCP) are reusing potentially contaminated FFRs and medical masks (MMs) on an  
14  
15 189 emergency basis due to supply shortages. These shortages have necessitated the rapid  
16  
17  
18 190 development and deployment of disinfection processes, leading to the World Health  
19  
20 191 Organization (WHO) issuing interim guidance on rational PPE use (1,2). The US Food and Drug  
21  
22  
23 192 Administration (FDA) granted Emergency Use Authorization of hydrogen peroxide and steam  
24  
25 193 sterilization systems to decontaminate FFRs for reuse (3). These technologies remain less  
26  
27  
28 194 available in low-resource settings, where frontline HCP have inadequate protection (4,5), thus  
29  
30 195 we need novel methods for PPE decontamination.

31  
32  
33 196 Photochemical disinfection uses a photosensitive chemical, which combined with visible  
34  
35 197 light generates singlet oxygen (Supplemental Section). Singlet oxygen inactivates viruses by  
36  
37  
38 198 damaging viral nucleic acids and membranes (6). One such photosensitizer is methylene blue  
39  
40 199 (MB), which is FDA-approved to treat methemoglobinemia, and used to sterilize human plasma  
41  
42 200 transfusions in Europe (7). MB inactivates SARS-CoV-2 and many other viruses (8-10)  
43  
44  
45 201 [Supplemental TABLE S3].

46  
47 202 This Development and Methods for N95 Respirators and Mask Decontamination  
48  
49  
50 203 (DeMaND) study aimed to evaluate methods that inactivate SARS-CoV-2 on respirators and  
51  
52 204 masks, which can be applied anywhere at low-cost. We examined if MB with light (MBL) could  
53  
54  
55 205 effectively decontaminate commonly-used FFRs and MMs while maintaining mask integrity  
56  
57 206 (filtration, breathability, fluid resistance and fit) after multiple decontamination cycles. We  
58  
59 207 leveraged four virology laboratories and six PPE integrity testing sites to examine: (a) MBL

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

208 virucidal effect on two SARS-CoV-2 isolates (*Betacoronavirus*) and two coronaviruses requiring  
209 a lower level of biocontainment (the *Betacoronavirus* murine hepatitis virus (MHV) and  
210 the *Alphacoronavirus* porcine respiratory coronavirus (PRCV)), and (b) the impact of five cycles  
211 of decontamination (5CD) on PPE integrity [FIGURE 1].

212 We selected the number of decontamination cycles based on the Centers for Disease  
213 Control and Prevention (CDC)'s recommended maximum number of donnings as part of crisis  
214 capacity strategies (11). We chose FFRs and MMs based on availability during recent outbreak  
215 responses and variations in shape, material and structure. For integrity testing, we compared  
216 MBL to the FDA-authorized vaporized hydrogen peroxide plus ozone system (VHP+O<sub>3</sub>) (2).

217  
**218 METHODS**

**219 Respirators and Masks**

220 We tested three FFRs and MM models, both fluid resistant and non-fluid resistant,  
221 [Supplemental Figure S9]. These FFRs are surgical FFRs: National Institute of Occupational  
222 Safety and Health (NIOSH)-approved particulate respirators FDA-cleared as medical devices.  
223 Supplemental TABLE S1 testing matrix.

**224 Viruses**

225 We obtained SARS-CoV-2 isolates from a patient at the George Washington University Hospital  
226 (Lab 1) and from Dr. Darryl Falzarano (VIDO) (GISAID accession ID: EPI\_ISL\_425177) (Lab  
227 2). We used a SARS-CoV-2 clinical sputum specimen with University of Calgary Conjoint  
228 Health Research Ethics Board approval (ID#REB20-0444). Recombinant MHV strain rA59-E-  
229 FL-M and PRCV strain 91V44 have been described previously (12-15).

**230 Virus Inoculation and Elution**

1  
2  
3 231 We cut FFRs and MMs into 7x10 mm coupons and inoculated them with the maximum available  
4  
5  
6 232 virus dose of SARS-CoV-2 or MHV on the outer layer (or inner layer where specified) with a  
7  
8 233 pipette and dried for 20 mins before treatment. Virus was eluted in media by vortex or orbital  
9  
10 234 rocker. Alternatively, we injected PRCV under the outer layer, and then we excised 34x34 mm  
11  
12  
13 235 coupons and vortexed in a media-containing tube. We quantified the remaining infectious virus  
14  
15 236 by median tissue culture infectious dose (TCID<sub>50</sub>) or plaque assays.

### 18 237 **Methylene Blue Treatment**

20 238 We added 10µM MB to the inoculated coupons or sprayed on intact inoculated masks, dried for  
21  
22  
23 239 30 minutes protected from light, and exposed to 50,000 lux of white light or 12,500 lux of red  
24  
25 240 light for 30 min. We used red light at a lower intensity because red light contains a higher  
26  
27  
28 241 percentage of wavelengths that activate MB. Dark controls were left in the biosafety cabinet with  
29  
30 242 the light off or covered by aluminum foil (<100 lux).

32  
33 243 For pre-treatment testing, we soaked R3 coupons with MB for >1 hour and dried 2 days  
34  
35 244 protected from light. We then spotted SARS-CoV-2 on outer or inner mask layers and dried for  
36  
37  
38 245 20 minutes before exposure to 50,000 lux of white light for 30 min. Intact RM and FW were  
39  
40 246 sprayed with 7-8mL MB and dried overnight. We added MHV to three points on the outer  
41  
42 247 surface, dried for 20 minutes, exposed to light (50,000 lux) for 30 min, excised the inoculated  
43  
44  
45 248 area, eluted, and quantified by TCID<sub>50</sub> assay.

### 47 249 **Light Sources**

49  
50 250 The Seattle Children's Research Institute, George Washington University, University of Calgary,  
51  
52 251 and Nelson Laboratories used lightboxes developed at Colorado State University and included  
53  
54 252 4000K Husky LED lights. The University of Alberta used 3500K Husky LEDs. The University  
55  
56  
57 253 of Liège and Centexbel used a custom lightbox containing horticultural lamps. All laboratories  
58  
59 254 verified light intensity using light meters [Supplemental Methods].  
60  
61  
62  
63  
64  
65



1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

255  
256  
257  
258  
259  
260  
261  
262  
263  
264  
265  
266  
267  
268  
269  
270  
271  
272  
273  
274  
275  
276  
277

**Integrity Testing**

We assessed respirator and mask integrity by determining filtration efficiency, breathability, fluid resistance and fit. We tested FFRs/MMs untreated and after 5CD with VHP+O<sub>3</sub> or 10μM MB plus white light (50,000 lux) or red light (12,500 lux) for 60 minutes. For the VHP+O<sub>3</sub> treatment, we used the pre-set cycle (Cycle 1) of Stryker’s STERIZONE VP4 Sterilizer at 41°C.

**Filtration Efficiency Testing**

We assessed filtration efficiency using NaCl sub-micron charged-neutralized particles ranging in size from 0.022–0.259μm with a median count diameter of 0.075 ± 0.020μm and a geometric standard deviation of less than 1.86 to give a mass median aerodynamic diameter of 0.3μm, with air flow at 85 L/min (simulating inhalation at heavy workload) (16). We measured bacterial filtration efficiency (BFE) of MMs using aerosolized droplets containing *Staphylococcus aureus* at a 28.3 L/min air flow rate (17,18) [Supplemental Methods and Results].

**Breathability Testing**

We assessed breathability by measuring inhalation and exhalation breathing resistances using standard test methods, and pressure drop measurements for MMs. Additionally, we determined Sheffield Dummy airflow differences for both FFRs and MMs [Supplemental Methods and Results].

**Fluid Resistance Testing**

Testing of resistance to splash and spray by synthetic blood is required for surgical masks in the US and fluid-resistant MMs in Europe. We tested fluid resistance for MMs [Supplemental Methods and Results].

**Fit Testing**

1  
2  
3 278 We conducted human fit testing with the PortaCount® Pro+ 8038 (TSI). Fit testing was  
4  
5  
6 279 exempted from ethics board review by both the Research Compliance Office, Stanford  
7  
8 280 University and the Conjoint Health Research Ethics Board, University of Calgary. We tested  
9  
10 281 multiple dynamic tasks: regular breathing, heavy breathing, turning head side-to-side, moving  
11  
12 282 head up-and-down, talking, and bending over breathing. We performed each set of tests twice  
13  
14 283 and calculated Fit Factor (FF) for each mask. We conducted Manikin fit testing using an  
15  
16 284 advanced, realistic manikin head and according to the NIOSH/National Personal Protective  
17  
18 285 Technology Laboratory (NPPTL) Decontaminated Respirator Assessment Plan (16). We  
19  
20 286 examined the changes in the elastic recovery of the FFR straps and MM ear loops to determine  
21  
22 287 changes in strap/ear loop integrity after 5CD [Supplemental Methods and Results].  
23  
24  
25  
26  
27

## 28 288 **Statistical Analysis**

29  
30 289 We calculated means and standard deviations or percent pass of each integrity test method  
31  
32 290 separately by FFR or MM model. We combined data for integrity test methods conducted at  
33  
34 291 more than one test site to create overall means and standard deviations or percent pass. We tested  
35  
36 292 normality of the data distribution using the Shapiro-Wilk test. We calculated significant  
37  
38 293 differences between untreated and treated FFRs and MMs with Student's t-tests, Mann-Whitney  
39  
40 294 U tests, or Fisher's exact tests (SAS v9.4) (19).  
41  
42  
43  
44

45 295

## 46 296 **RESULTS**

### 47 297 **Methylene blue and light (MBL) tissue culture plate inactivation**

48  
49  
50 298 To confirm that MBL can inactivate a coronavirus, varying concentrations of MB were mixed  
51  
52 299 with PRCV and exposed to red light (12,500 lux). Treatment with 0.1µM MB plus light resulted  
53  
54 300 in complete inactivation. In the absence of additional light, complete inactivation required a dose  
55  
56 301 1µM MB [FIGURE 2A].  
57  
58  
59  
60  
61  
62  
63  
64  
65

1  
2  
3 302 To confirm the ability of MBL to specifically reduce SARS-CoV-2 infectivity, varying  
4  
5  
6 303 concentrations of MB were mixed with SARS-CoV-2 and exposed to 50,000 lux of white light.  
7  
8 304 MB inhibited SARS-CoV-2 infectivity with a dose-dependent effect, with or without exposure to  
9  
10 305 light. This virucidal effect was enhanced in the presence of light [FIGURE 2B].  
12

### 13 306 **MBL FFR and MM material inactivation**

14  
15 307 To examine the MBL dose required to decontaminate FFR and MM material inoculated with  
16  
17  
18 308 SARS-CoV-2 or MHV, we cut coupons from a representative FFR (R3) or MM (FW) and  
19  
20 309 inoculated and treated with MBL for the indicated time periods. Both viruses displayed  
21  
22  
23 310 sensitivity to MBL treatment. Using 10 $\mu$ M MB and light resulted in complete inactivation of  
24  
25 311 SARS-CoV-2 and MHV on both FFR and MM materials after 5 minutes [FIGURE 3A]. Using  
26  
27 312 1 $\mu$ M MB, we observed complete inactivation after 30 minutes of light exposure, though we  
28  
29 313 observed a 2-4 log viral titer reduction after 5 minutes. MB treatment in the absence of additional  
30  
31 314 light also resulted in substantial reduction of viral titers.  
32

33  
34  
35 315 To ensure that MBL can efficiently decontaminate a variety of masks, we tested three  
36  
37 316 more masks, including two additional FFRs (RH) and (RM), and one additional MM (FH). We  
38  
39 317 inoculated coupons or intact masks, treated with 10 $\mu$ M MB and exposed to light for 30 minutes  
40  
41 318 [FIGURE 3B-E], conditions which demonstrated robust inactivation in the previous experiment.  
42  
43 319 We observed complete inactivation (up to 4 logs) of SARS-CoV-2 for all respirators and masks  
44  
45 320 tested. Treatment with MB without exposure to white light resulted in substantial virus reduction  
46  
47 321 [FIGURE 3D]. We observed complete inactivation (4-5 log reduction) of MHV for FH, R3, RH,  
48  
49 322 and RM masks. A low level of virus was detectable in one replicate for FW [FIGURE 3B]. For  
50  
51 323 PRCV, which was injected under the outer mask layer, we observed a >5-log virus reduction  
52  
53 324 after treatment of FH, FW, R3 and RH masks. In contrast, we observed a 3-log reduction in RM  
54  
55 325 [FIGURE 3E]. The overall percent reduction in virus titer after treatment across all FFRs/MMs  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

1  
2  
3 326 and viruses ranged from 99.8->99.9% [TABLE 1]. In addition, we tested the effect of MBL  
4  
5  
6 327 inactivation on FFR and MM straps inoculated with PRCV and noted 2-4 log reduction in titers  
7  
8 328 [Supplemental FIGURE S4].  
9

### 10 329 **Evaluation of Potential Applications of MBL in a Clinical Setting**

11  
12  
13 330 We examined three potential applications of MBL in a clinical environment. First, since some  
14  
15 331 clinical settings may not have access to bright light, we investigated whether 10 $\mu$ M MB and  
16  
17  
18 332 ambient light would be sufficient to inactivate SARS-CoV-2. MB treatment and exposure to 700  
19  
20 333 lux (ambient light generated by light in a biosafety cabinet) for 60 minutes inactivated nearly 5-  
21  
22  
23 334 logs of SARS-CoV-2. MB and <100 lux of light inactivated almost 3-logs of virus [FIGURE  
24  
25 335 4A].  
26

27  
28 336 Second, we investigated the possibility of pre-treating respirators or masks with MB. We  
29  
30 337 treated coupons with 10 $\mu$ M MB, dried overnight, and inoculated them with SARS-CoV-2 on  
31  
32  
33 338 either the hydrophobic outer layer or the hydrophilic inner layer before exposure to 50,000 lux of  
34  
35 339 white light for 30 min. We could not recover infectious virus from either side of the light-  
36  
37  
38 340 exposed coupons, signifying inactivation of >4 logs of virus [FIGURE 4B]. We sprayed intact  
39  
40 341 RM respirators and FH masks with 10 $\mu$ M MB, dried overnight, inoculated with MHV, and  
41  
42  
43 342 exposed to 50,000 lux of white light for 30 min. No viable virus was recovered. [FIGURE 4D].  
44

45 343 Lastly, we added 10 $\mu$ l of a clinical specimen (saliva) with a titer of  $1.15 \times 10^5$  PFU/ml  
46  
47 344 obtained from a COVID-19 patient onto respirator coupons, and treated with 10 $\mu$ M MB and  
48  
49  
50 345 white light (50,000 lux) for 30 min. No viable virus was detected post-treatment, thus indicating  
51  
52 346 the potential for this inactivation method in clinical settings in which viable virus may be  
53  
54  
55 347 protected by proteinaceous matrixes [FIGURE 4C].  
56

### 57 348 **Integrity Testing**

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

349 We employed standard test methods to examine if MBL decontamination affected integrity and  
350 compared results to the FDA-authorized VHP+O<sub>3</sub> decontamination method. The following  
351 sections describe each of the integrity test methods and results [Supplemental TABLES S2A-B  
352 for complete results]. Additional testing for MMs included bacterial filtration efficiency,  
353 differential pressure, Sheffield dummy, fluid resistance, and strap/ear loop integrity testing  
354 [Supplemental FIGURES S5-S8].

355 Filtration Efficiency

356 FIGURE 5A depicts the filtration efficiency before (untreated) and after 5CD. We expected high  
357 filtration efficiencies for the FFRs as they are all NIOSH-approved N95 FFRs, which requires  
358  $\geq 95\%$  sub-micron filtration efficiency. All FFR models surpassed the minimum 95% filtration  
359 efficiency requirement before and after 5CD. Untreated FW and FH masks achieved 76% and  
360 86% filtration efficiency, respectively. Overall, MBL and VHP+O<sub>3</sub> treatment of FFRs and MMs  
361 did not cause any significant differences in the filtration efficiency of the studied models  
362 ( $p > 0.01$ ). MM models continued to meet requirements of differential pressure after 5CD  
363 [Supplemental FIGURE S5 and TABLE S2A].

364 Breathability

365 The resistance to airflow via inhalation and exhalation (breathability), is an indication of the  
366 difficulty in breathing through the respirators or masks. The FFR models achieved  
367 inhalation/exhalation resistances  $> 60\%$  below respective NIOSH 42 CFR Part 84 and EN 149  
368 requirements after 5CD [FIGURE 5B, C]. These resistance changes would not make it harder to  
369 breathe through the mask. MMs demonstrated similar inhalation resistances, and lower  
370 exhalation resistance values compared to FFRs after 5CDs. Both MM models were below their  
371 respective allowable maximum differential pressure limit after 5CD [Supplemental FIGURE S6  
372 and TABLE S2A]. Furthermore, we determined air flow differences using the Sheffield Dummy

1  
2  
3 373 [Supplemental FIGURE S7 and TABLE S2A-B]. The MBL treatment did not affect the  
4  
5  
6 374 breathability of FFRs or MMs, in terms of either inhalation and exhalation resistances or  
7  
8 375 pressure drop, respectively.  
9

#### 10 376 Fluid Resistance

11  
12  
13 377 We evaluated MMs for their fluid resistance and found them to be resistant when challenged  
14  
15 378 from the outside (conventional challenge direction) but less so from the inside of the mask  
16  
17  
18 379 [Supplemental FIGURE S8 and TABLE S2A].  
19

#### 20 380 Fit Testing

21  
22  
23 381 Fit testing measures how well a respirator or mask seals around the contours of the face. A good  
24  
25 382 fit ensures exchanged air is filtered through the respirator. Human fit testing demonstrated that  
26  
27 383 respirators maintained quantitative fit values, or fit factors (FF), above 100 after 5CD. In  
28  
29  
30 384 contrast, VHP+O<sub>3</sub> decontamination decreased RH and RM fit to the point of failure [FIGURE  
31  
32  
33 385 6A]. Note that two VHP+O<sub>3</sub> decontamination cycles is the maximum authorized by FDA for  
34  
35 386 N95 FFRs (20). We also performed human fit testing for the MMs to demonstrate that these  
36  
37 387 types of masks are not designed to ensure a tight fit [FIGURE 6A]. On some of the VHP+O<sub>3</sub>-  
38  
39  
40 388 treated FFRs and MMs, human participants noted a “strong acrid odor” and some observed  
41  
42 389 partial elasticity loss on treated straps and ear loops, and discoloration of the nosepiece foams  
43  
44  
45 390 (RM only). In contrast, some participants wearing the MBL-treated FFRs noted a “not  
46  
47 391 unpleasant slight odor” at one of the fit testing sites. In addition to the discoloration, the nose  
48  
49  
50 392 bridge was more rigid for the three MBL-treated RMs.  
51

52 393 We determined Manikin FF using an advanced, realistic manikin headform which  
53  
54 394 resulted in similar overall passing of OSHA criterion of 100 FF for all three FFRs [FIGURE  
55  
56  
57 395 6B](16,21). Observed differences between human and manikin fit can be attributed to testing  
58  
59 396 procedure variability and structural facial variations. FFRs do not provide a universal fit for all  
60  
61  
62  
63  
64  
65

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

397 wearers. Overall, MBL decontamination after 5CD did not negatively impact integrity  
398 performance and fit while the VHP+O<sub>3</sub> decontamination yielded some detrimental performance  
399 issues.

400  
401 **DISCUSSION**

402 We demonstrate that MB activated by white or red light effectively inactivates SARS-CoV-2 on  
403 FFR and MM surfaces, and with a clinical specimen, without affecting integrity or fit. MBL can  
404 be applied as a decontamination method for single-use FFRs and MMs. Residual MB on the  
405 mask surface could potentially provide a novel means of continual inactivation of viral particles  
406 to decontaminate a mask while donned, since even under ambient light conditions, MB  
407 inactivated SARS-CoV-2 on mask surfaces. .

408 For decades, MB has been recognized to have disinfection capabilities against a range of  
409 viral and bacterial pathogens (7-9,22), and MB is currently used to sterilize plasma for  
410 transfusion (23)and to sterilize convalescent serum for COVID-19 treatment (10).

411 MBL is suitable for high- and low-resource settings since MB is inexpensive, globally  
412 available, and does not require specialized equipment. Light sources can vary from white high-  
413 intensity lamps to ambient lighting to generate singlet oxygen [Supplemental TABLE S6].  
414 Future studies are warranted to investigate whether MBL could be used to inactivate additional  
415 pathogens and decontaminate other forms of PPE such as gowns, gloves, and boots.

416 One limitation was that we only tested a minority of FFR and MM models, yet there are  
417 approximately 500 NIOSH-approved FFR models, and many others used globally. MBL worked  
418 well on all FFRs and MMs tested, except the “RM” FFR possibly owing to a distinct design  
419 characteristic which resulted in the variable outcome. CDC recommends that a decontamination

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

420 method's effectiveness be evaluated for specific FFR models in collaboration with the  
421 manufacturer, and if needed, a third-party laboratory (25).

422         During our integrity testing, we did not simulate extended wear or multiple donnings and  
423 doffings, which could affect FFR fit and performance (26,27). In addition, off-gassing of MB or  
424 VHP+O<sub>3</sub> was not evaluated. The biocompatibility of MB wearer inhalation was not tested,  
425 however, MB concentrations used were below those administered clinically (intravenously,  
426 orally or intranasally) (7,28,29). If the entire dose of 10µM MB sprayed onto a mask was  
427 inhaled, which is unlikely, the total inhaled dosage would be 0.02 mg. The quantity of MB  
428 inhalation overtime while wearing a MB-pretreated mask is under investigation.

429         We generalized our findings by demonstrating complete MBL inactivation employing the  
430 same methodology across multiple virology laboratories using three coronavirus species and a  
431 SARS-CoV-2 clinical sample. This signifies that emergent variants of SARS-CoV-2 would also  
432 be inactivated by MBL and that viruses requiring lower levels of biocontainment can be used for  
433 similar inactivation studies. Integrity tests in multiple testing centers using heterogeneous light  
434 administration methods reaffirms the reproducibility of our findings and we replicated practical  
435 light scenarios expected in the real-world settings.

436         In conclusion, MBL treatment inactivates SARS-CoV-2 on FFRs and MMs without  
437 decreasing integrity and fit. Our findings provide a method for inexpensive, accessible, effective  
438 decontamination of PPE for reuse, applicable in high- and low-resource settings during supply  
439 shortages. Pretreatment of masks with MB could provide a novel means of continual disinfection  
440 reducing exposure to SARS-CoV-2.



1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

444  
445  
446  
447  
448  
449  
450  
451  
452  
453  
454  
455  
456  
457  
458  
459  
460  
461  
462  
463  
464  
465  
466  
467

**Financial Support**

This work was supported by an Amazon Catalyst Award through the University of Washington [TSL]; an Anonymous Donor to the Department of Urology, University of Washington [TSL]; Open Philanthropy [MC], Alberta Health Services [JC, DE], The Li Ka Shing Institute of Virology [DE/JC].

**Conflict of Interest**

*Potential conflicts of interest.* TSL, JC and TC are co-founders of Singletto, Inc. DE has stock investment in Singletto, Inc. YC, SC are co-founders of 4C Air, Inc. MZ and LL are employees of 4C Air, Inc. JMC has received research funding from Pfizer. MC received funding from BMGF.

*No conflict.* BHH, FEMS, FSK, YLL, MML, LFC, AP, YCL, CNM, JS, KBK, EH, ET, BH, JL, SS, JMD, TW, TC, SJS, RP, TG, ET, LLB, MN, CM, KH, KP, SR, PF, OJ, AP, JLL, V<S. KH, SRT, CW, MM, RM, JFW, HN, LD, SdeJ.

**Acknowledgements**

We all thank the human fit testing participants and the patients from whom the original SARS-CoV-2 specimens were obtained which were used for the virology testing. MCC thanks the contribution of the NIOSH National Personal Protective Technology Laboratory: Jonisha P. Pollard, Michael S Bergman, Kevin Strickland, Rebecca Streeter, Christian C. Coby, Nichole Suhon, and Jeremy J Brannen. BHH and MCC acknowledge the biomedical engineering

1  
2  
3 468 hackathon group through Cassandra Howard and the light boxes built by the Colorado State  
4  
5  
6 469 University Biomedical team, Dr. Jorge Rocca and Han Chi. DE wishes to thank Megan  
7  
8 470 Desaulniers and Dr. Dan Dragon for BSL3 operations at the University of Alberta. JMC  
9  
10 471 acknowledges the assistance of Johanna Blaak and Michelle Wright of the W21C Research and  
11  
12  
13 472 Innovation Centre, University of Calgary for consultation on methodology and for project  
14  
15 473 management, respectively, Jeanette Adams and Rhea Campbell of Alberta Health Services for  
16  
17  
18 474 conducting the human fit testing, and David Silverstone from Alberta Health Services for  
19  
20  
21 475 oversight and management. Stanford AIM lab gratefully acknowledges the contributions of our  
22  
23 476 Stanford Science, Technology and Medicine Research Interns in the development of the fit  
24  
25 477 questionnaire assessment and the human fit volunteer participants. ET wishes to thank Amélie  
26  
27  
28 478 Matton, Murielle Perrin and Frédéric de Meulemeester (AMB Ecosteryl, Mons, Belgium), for  
29  
30 479 suggestions and technical and administrative support and thanks Chantal Vanmaercke and Carine  
31  
32  
33 480 Boone for their excellent technical support. MCC thanks the administrative support of Mary  
34  
35 481 Moua. TSL acknowledges the support of Drs. Danielle Zerr, Ruth MacDonald, and Paul  
36  
37  
38 482 Merguerian at Seattle Children’s Hospital. FSKB and YLL acknowledge the donation of masks  
39  
40 483 and respirators from the WHO, 3M and Halyard, as well as the guidance from the WHO Clinical  
41  
42 484 Diagnostics Group (CDG) and the Infection Prevention and Control (IPC) group.  
43  
44  
45 485

46  
47 **Disclaimer**  
48

49  
50 487 *The findings and conclusions in this report are those of the authors and do not necessarily*  
51  
52 488 *represent the official position of the Centers for Disease Control and Prevention.*  
53

54  
55 489  
56  
57 490  
58

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

**REFERENCES**

- 491 1. WHO. Rational use of personal protective equipment for coronavirus disease 2019 (COVID-  
492 19). World Health Organization, 2020; 27:1–7.
- 493 2. United States Food and Drug Administration. Decontamination Systems for Personal  
494 Protective Equipment EUAs, 2020; 1–4. Available from: [https://www.fda.gov/medical-](https://www.fda.gov/medical-devices/coronavirus-disease-2019-covid-19-emergency-use-authorizations-medical-devices/decontamination-systems-personal-protective-equipment-euas)  
495 [devices/coronavirus-disease-2019-covid-19-emergency-use-authorizations-medical-](https://www.fda.gov/medical-devices/coronavirus-disease-2019-covid-19-emergency-use-authorizations-medical-devices/decontamination-systems-personal-protective-equipment-euas)  
496 [devices/decontamination-systems-personal-protective-equipment-euas](https://www.fda.gov/medical-devices/coronavirus-disease-2019-covid-19-emergency-use-authorizations-medical-devices/decontamination-systems-personal-protective-equipment-euas) (accessed 12/20/2020)
- 497 3. Battelle. Final Report for the Bioquell Hydrogen Peroxide Vapor (HPV) Decontamination for  
498 Reuse of N95 Respirators. 2016; 46.
- 499 4. Burki, Talha. Global shortage of personal protective equipment.  
500 *Lancet Inf Dis* 2020; 20:785-786. doi.org/10.1016/S1473-3099(20)30501-6
- 501 5. Nkengasong, JN, Mankoula W. Looming threat of COVID-19 infection in Africa: act  
502 collectively, and fast. *Lancet* 2020; 395:841-2. doi.org/10.1016/S0140-6736(20)30464-5
- 503 6. Costa L, Faustino MAF, Neves MGPMS, Cunha Â, Almeida A. Photodynamic inactivation of  
504 mammalian viruses and bacteriophages. *Viruses* 2012; 4:1034–74.
- 505 7. Seghatchian J, Walker WH, Reichenber S: Updates on pathogen inactivation of plasma using  
506 Theraflex methylene blue system. *Transfus Apher Sci* 2008; 38:271–80.
- 507 8. Eickmann M, Gravemann U, Handke W, Tolksdorf F, Reichenberg S, Müller TH, et al.  
508 Inactivation of Ebola virus and Middle East respiratory syndrome coronavirus in platelet  
509 concentrates and plasma by ultraviolet C light and methylene blue plus visible light, respectively.  
510 *Transfusion* 2018; 58:2202–7.
- 511 9. Eickmann M, Gravemann U, Handke W, Tolksdorf F, Reichenberg S, Müller TH, et al.  
512 Inactivation of three emerging viruses – severe acute respiratory syndrome coronavirus,  
513 Crimean–Congo haemorrhagic fever virus and Nipah virus – in platelet concentrates by

1  
2  
3 515 ultraviolet C light and in plasma by methylene blue plus visible light. *Vox Sanguinis* 2020;  
4  
5  
6 516 115:146–51.  
7  
8 517 10. Duan K, Liu B, Li C, Zhang H, Yu T, Qu J, et al. Effectiveness of convalescent plasma  
9  
10 518 therapy in severe COVID-19 patients. *Proceedings of the National Academy of Sciences* 2020;  
11  
12  
13 519 117:9490-6.  
14  
15  
16 520 11. Bergman MS, Viscusi DJ, Heimbuch BK, Wander JD, Sambol AR, Shaffer RE. Evaluation  
17  
18 521 of multiple (3-Cycle) decontamination processing for filtering facepiece respirators. *Journal of*  
19  
20  
21 522 *Engineered Fibers and Fabrics* 2010; 5:33–41.  
22  
23 523 12. Boscarino JA, Logan HL, Lacny JJ, Gallagher TM. Envelope protein palmitoylations are  
24  
25 524 crucial for murine coronavirus assembly. *Journal of Virology* [Internet] 2008; 82:2989–99.  
26  
27  
28 525 Available from: <http://www.ncbi.nlm.nih.gov/pubmed/18184706>  
29  
30 526 13. Pensaert M, Callebaut P, Vergote J. Isolation of a porcine respiratory, non-enteric  
31  
32  
33 527 coronavirus related to transmissible gastroenteritis. *The Veterinary Quarterly* 1986; 8:257–61.  
34  
35 528 14. Wesley RD, Hill HT, Biwer JD. Evidence for a porcine respiratory coronavirus, antigenically  
36  
37  
38 529 similar to transmissible gastroenteritis virus, in the United States. Vol. 2, *Journal of Veterinary*  
39  
40 530 *Diagnostic Investigation* 1990. p. 312–7.  
41  
42  
43 531 15. Cox E, Hooyberghs J, Pensaert MB. Sites of replication of a porcine respiratory coronavirus  
44  
45 532 related to transmissible gastroenteritis virus. *Research in Veterinary Science* 1990;48:165–9.  
46  
47  
48 533 16. NIOSH. Decontaminated Respirator Assessment Plan. NIOSH. 2020. Available from:  
49  
50 534 [https://www.cdc.gov/niosh/npptl/respirators/testing/pdfs/NIOSHApproved\\_Decon\\_TestPlan10.p](https://www.cdc.gov/niosh/npptl/respirators/testing/pdfs/NIOSHApproved_Decon_TestPlan10.pdf)  
51  
52 535 [df](https://www.cdc.gov/niosh/npptl/respirators/testing/pdfs/NIOSHApproved_Decon_TestPlan10.pdf) (accessed 12/20/2020)  
53  
54  
55 536 17. ASTM International. 2019. ASTM F2100-19e1: Standard Specification for Performance of  
56  
57 537 Materials Used in Medical Face Masks.  
58  
59  
60  
61  
62  
63  
64  
65

1  
2  
3 538 18. EN 14683:2019, Medical face masks. Requirements and test methods.  
4  
5  
6 539 <https://www.nelsonlabs.com/wp-content/uploads/2018/07/Face-Masks-2019.pdf> (accessed  
7  
8 540 12/20/2020)  
9  
10  
11 541 19.[http://documentation.sas.com/?cdcId=pgmsascdc&cdcVersion=9.4\\_3.4&docsetId=pgmsasho](http://documentation.sas.com/?cdcId=pgmsascdc&cdcVersion=9.4_3.4&docsetId=pgmsasho)  
12  
13 542 [me&docsetTarget=home.htm&locale=en](http://documentation.sas.com/?cdcId=pgmsascdc&cdcVersion=9.4_3.4&docsetId=pgmsasho&docsetTarget=home.htm&locale=en) (accessed 12/20/2020).  
14  
15  
16 543 20. FDA letter, June 6, 2020, <https://www.fda.gov/media/136976/download> (accessed  
17  
18 544 12/20/2020).  
19  
20  
21 545 21. Bergman MS, Zhuang Z, Hanson D, Heimbuch BK, McDonald MJ, Palmiero AJ, et al.  
22  
23 546 Development of an advanced respirator fit-test headform. *Journal of Occupational and*  
24  
25 547 *Environmental Hygiene* 2014; 11:117-125.  
26  
27  
28  
29 548 22. Perdrau JR Charles T. The photodynamic action of methylene blue on bacteriophage. *Proc.*  
30  
31 549 *R. Soc. Lond* 1933; 112277–287; <http://doi.org/10.1098/rspb.1933.0010>  
32  
33  
34 550 23. Organización Mundial de la Salud (OMS). World health organization model list of essential  
35  
36 551 medicines. *Mental and Holistic Health: Some International Perspectives*. 2019; 21:119–34.  
37  
38  
39 552 25. CDC. Implementing Filtering Facepiece Respirator (FFR) Reuse, Including Reuse after  
40  
41 553 Decontamination, When There Are Known Shortages of N95 Respirators. CDC. 2020. Available  
42  
43 554 from: [https://www.cdc.gov/coronavirus/2019-ncov/hcp/ppe-strategy/decontamination-reuse-](https://www.cdc.gov/coronavirus/2019-ncov/hcp/ppe-strategy/decontamination-reuse-respirators.html)  
44  
45 555 [respirators.html](https://www.cdc.gov/coronavirus/2019-ncov/hcp/ppe-strategy/decontamination-reuse-respirators.html) (accessed 12/20/2020)  
46  
47  
48  
49 556 26. Degesys NF, Wang RC, Kwan E, Fahimi J, Noble JA, Raven MC. Correlation Between N95  
50  
51 557 Extended Use and Reuse and Fit Failure in an Emergency Department. *JAMA [Internet]* 2020;  
52  
53 558 324:94. Available from: <https://jamanetwork.com/journals/jama/fullarticle/2767023>  
54  
55  
56 559 27. Lieu A, Mah J, Zanichelli V, Exantus RC, Longtin Y. Impact of extended use and  
57  
58 560 decontamination with vaporized hydrogen peroxide on N95 respirator fit. *Am J Infect Control*

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

561 2020; 48:1457-1461. doi: 10.1016/j.ajic.2020.08.010. Epub 2020 Aug 15.

562 28. Rengelshausen J, Burhenne J, Fröhlich M, Tayrouz Y, Singh SK, Riedel KD, et al.

563 Pharmacokinetic interaction of chloroquine and methylene blue combination against malaria.

564 *European Journal of Clinical Pharmacology* 2004;60:709–15.

565 29. Krespi YP, Kizhner V. Laser-assisted nasal decolonization of *Staphylococcus aureus*,

566 including methicillin-resistant *Staphylococcus aureus*. *American Journal of Otolaryngology -*

567 *Head and Neck Medicine and Surgery* [Internet] 2012; 33:572–5. Available from:

568 <http://dx.doi.org/10.1016/j.amjoto.2012.02.002>

569  
570  
571

1  
2  
3 572  
4  
5  
6 573  
7 574  
8 575  
9 576

**Table 1: Virus Reduction by 10 µM Methylene Blue with Light**

Mask	MHV		<sup>b</sup> PRCV		Lab 1 SARS-CoV-2		Lab 2 SARS-CoV-2		Avg. SARS-CoV-2		Overall avg.	
	Log reduction	% Inactivation	Log reduction	% Inactivation	Log reduction	% Inactivation	Log reduction	% Inactivation	Log reduction	% Inactivation	Log reduction	% Inactivation
<b>RH</b>	4.4	>99.9%	5.5	>99.9%	2.2	>99.4%	4.3	>99.9%	3.2	99.6%	4.1	99.8%
<b>RM</b>	3.5	>99.9%	2.7	99.8%	2.8	>99.8%	4.0	>99.9%	3.4	99.9%	3.2	99.9%
<b>R3</b>	5.1	>99.9%	5.0	>99.9%	<sup>a</sup> 3.3	>99.9%	3.1	>99.9%	3.2	>99.9%	4.1	>99.9%
<b>FW</b>	5.8	>99.9%	5.5	>99.9%	<sup>a</sup> 3.6	>99.9%	3.1	>99.9%	3.4	>99.9%	4.5	>99.9%
<b>FH</b>	3.8	>99.9%	5.1	>99.9%	3.1	>99.9%	4.2	>99.9%	3.6	>99.9%	4.0	>99.9%

<sup>a</sup>Data extracted from inactivation curve.

<sup>b</sup>Light source for testing MB on PRCV = 12500 lux red light; Light source for testing MB on all other virus types = 50000 lux white light.

Due to the limit of detection of the assays used to titer the virus, the highest % inactivation is indicated as >99.9%.

Abbreviations: RH, Halyard duckbill respirator (Fluidshield-46727); RM, 3M half-sphere respirator (1860); R3, 3M

Panel respirator (1870+);

FW, Type II EN14 683 generic face mask; FH, Type II RASTM F2100 Level 2 Halyard face mask.

43 577  
44 578  
45 579

1  
2  
3  
4 580 **Figure legends**

5  
6 581 **FIGURE 1. Graphical representation of the DeMaND study methodology.** (A) Overview of the  
7  
8 582 coronaviruses, respirators, masks and decontamination methods used. (B) FFRs and MMs were  
9  
10 583 inoculated with virus and treated with MB and light (MBL). Remaining infectious virus was  
11  
12  
13 584 quantified using TCID<sub>50</sub> or plaque assay. (C) In parallel with the virucidal testing of MBL, intact  
14  
15 585 FFRs and MMs were subjected to 5 cycles of decontamination before mask integrity was tested  
16  
17  
18 586 using the indicated methods. PRCV = porcine respiratory coronavirus, SARS-CoV-2 = severe  
19  
20 587 acute respiratory syndrome coronavirus 2, MHV = murine hepatitis virus, MBL = methylene  
21  
22  
23 588 blue + light, VHP+O<sub>3</sub> = vaporized hydrogen peroxide plus ozone. See Supplemental Table S1  
24  
25 589 for the respirator and mask decontamination and testing matrix.

26  
27  
28 590 **FIGURE 2. Inactivation of PRCV and SARS-CoV-2 using methylene blue and light**

29  
30 591 (MBL). (A) To determine the efficacy of different MB concentrations, we added serial dilutions  
31  
32  
33 592 of MB to wells of a 48-well plate containing 10 µL PRCV (2x10<sup>7</sup> TCID<sub>50</sub>/ml). Plates were either  
34  
35 593 exposed to red light (12,500 lux) for 30 minutes or were protected from light (<100 lux). Dotted  
36  
37  
38 594 line indicates limit of detection. (B) We added serial dilutions of MB to wells of a 12-well plate  
39  
40 595 containing ~50 PFU of SARS-CoV-2 in MEM plus 15% FCS. Plates were either exposed to white  
41  
42 596 light (50,000 lux) for 45 min or protected from light (<100 lux). We determined viral titers using  
43  
44  
45 597 2-3 replicate samples. ND= not detected.

46  
47 598 **FIGURE 3. MBL inactivates MHV, SARS-CoV-2, and PRCV on FFR and MM material.** (A)

48  
49  
50 599 Effect of methylene blue and light treatment on MHV and SARS-CoV-2 titers. We applied a 10 µl  
51  
52 600 aliquot of MHV or SARS-CoV-2 to coupons derived from a FFR (R3) or MM (FW) and they were  
53  
54  
55 601 left to dry for 20 min. Subsequently, we added 10 or 30 µl of MB to each coupon at the indicated  
56  
57 602 concentrations. We exposed the samples to white light (50,000 lux) for the indicated time periods  
58  
59  
60 603 or left them in the biosafety cabinet with the lights off. We measured each virus titer using 2-6



1  
2  
3 604 replicate samples by TCID<sub>50</sub> or plaque assay. . **(B-D)** We applied a 10 µl aliquot of SARS-CoV-2  
4  
5  
6 605 or MHV to coupons of the indicated masks and dried for 20 min. Depending on coupon size, we  
7  
8 606 added 10-30 µl of 10 µM MB to each coupon, and treated the samples with light (50,000 lux) or  
9  
10 607 protected them from light. **(E)** We injected 100 µl of PRCV under the outer layer of intact MMs  
11  
12 608 or FFRs and allowed them to dry for 30 minutes. Subsequently, we sprayed the FFRs and MMs  
13  
14 609 with 10 µM MB and dried them for 30 minutes in the dark before exposure to red light (12,500  
15  
16 610 lux). We determined each virus titer using 2-6 replicate samples by TCID<sub>50</sub> or plaque assay. Data  
17  
18 611 is represented as mean +/- SD. ND = Not detected. RH= Halyard duckbill respirator  
19  
20  
21  
22 612 (Fluidshield-46727). RM= 3M half-sphere respirator (1860). R3= 3M panel respirator (1870+).  
23  
24 613 FW= Type II EN 14683 generic face mask. FH= Type IIR ASTM F2100 Level 2 Halyard face  
25  
26 614 mask. Dotted line indicates limit of detection.  
27  
28  
29

30 **FIGURE 4. Potential applications of MBL in a clinical setting.** **(A)** Effect of low light levels on  
31  
32 615 SARS-CoV-2 inactivation using MB. We applied a 10 µl aliquot of SARS-CoV-2 to R3 coupons  
33  
34 616 and dried for 20 min. We added 10 µL of 10 µM MB to each coupon before treatment with 700  
35  
36 617 lux or <100 lux of light (the light level produced by the biosafety hood lights). **(B)** Effect of MB  
37  
38 618 pre-treatment on SARS-CoV-2 inactivation. We cut coupons from R3 masks and soaked for 1 hr  
39  
40 619 in 10 µM MB. We then dried the coupons in the dark for 2 days before adding 10 µl of virus to  
41  
42 620 either the inner or outer layers. We exposed the samples to white light (50,000 lux) for 30 min  
43  
44 621 and determined the virus titer by plaque assay. **(C)** Inactivation of a SARS-CoV-2 clinical  
45  
46 622 specimen by MBL. We obtained a saliva specimen from a COVID-19 patient with a titer of 1.1 x  
47  
48 623 10<sup>5</sup> PFU/ml for SARS-CoV-2. We applied 10 µl aliquots to coupons cut from a R3 mask and  
49  
50 624 treated with 10 µM MB and exposed to white light (50,000 lux) for 30 min. We determined virus  
51  
52 625 titer by plaque assay. **(D)** Effect of MB pre-treatment on MHV inactivation using intact masks.  
53  
54 626 We pretreated intact R3 and FW masks with 10 µM MB by spraying the front and back with a  
55  
56 627  
57  
58  
59  
60  
61  
62  
63  
64  
65

1  
2  
3  
4 628 total of 7-8 ml of MB and allowing to dry overnight in the dark. We inoculated the dried masks  
5  
6 629 with MHV and exposed to white light (50,000 lux) for 30 minutes. We then excised inoculated  
7  
8 630 areas before elution and titration. We determined virus titer by TCID<sub>50</sub> assay. ND = Not  
9  
10 631 detected. RM= 3M 1860 half-sphere respirator. FH= Type IIR Halyard face mask. Dotted line  
11  
12  
13 632 indicates limit of detection.

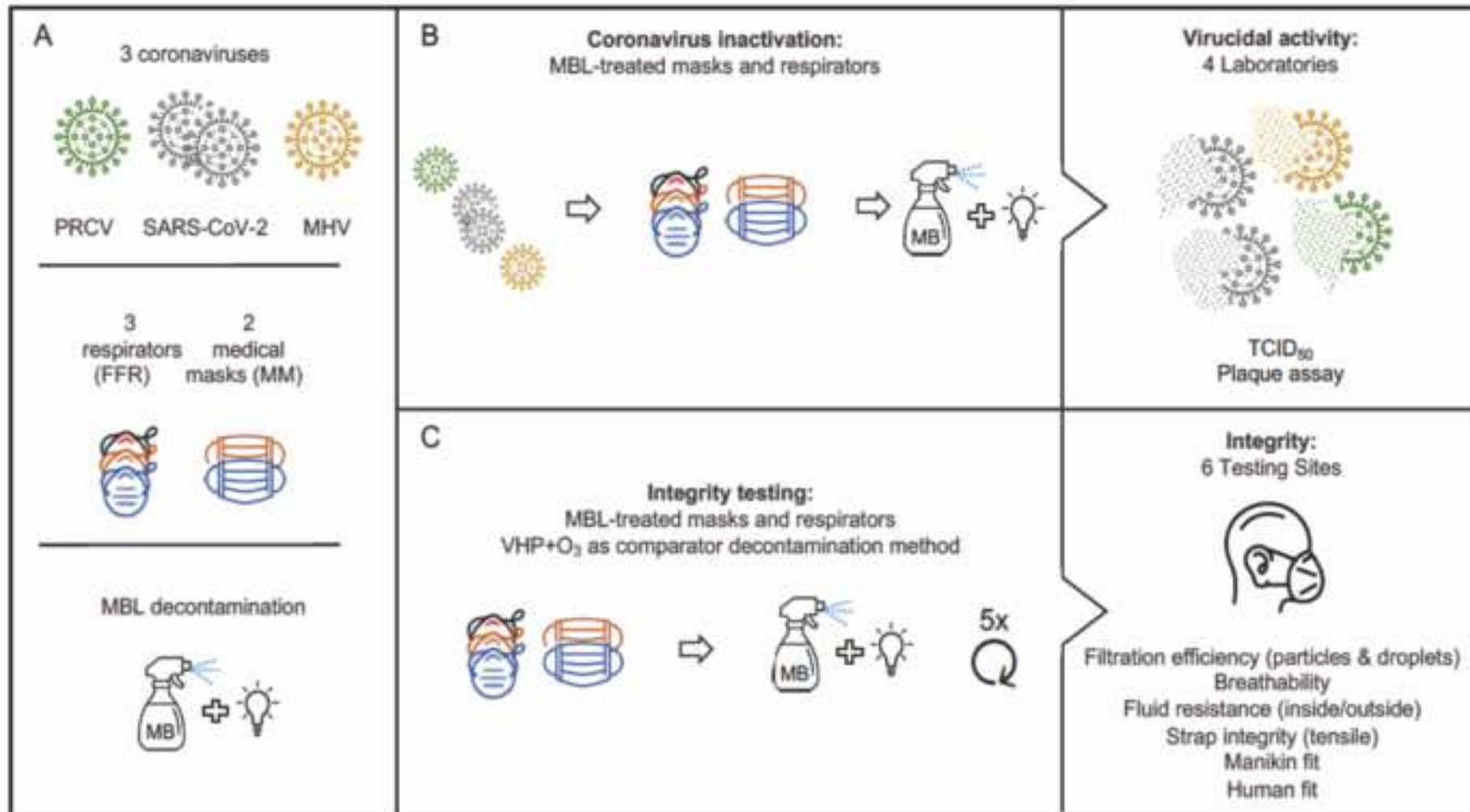
14  
15  
16 633 **FIGURE 5. Effect of MBL and VHP+O<sub>3</sub> treatments on NaCl sub-micron filtration efficiencies**

17  
18 634 **and breathability before and after 5CD. (A)** NaCl sub-micron filtration efficiency is a measure  
19  
20 635 of the ability of an FFR or MM to capture aerosolized particles smaller than one micron,  
21  
22  
23 636 expressed as a percentage of particles that do not pass the material at a given velocity or flow  
24  
25 637 rate. **(B)** Inhalation and **(C)** exhalation breathing resistances before and after 5CD. The  
26  
27 638 resistance to airflow during inhalation and exhalation is an indication of the difficulty in  
28  
29  
30 639 breathing through the respirators/masks. \*Results from decontaminated FFRs and MMs are  
31  
32  
33 640 significantly different from untreated masks (Student's t test or Mann-Whitney U test  
34  
35 641  $p < 0.01$ ). RH= Halyard duckbill respirator (Fluidshield-46727). RM= 3M half-sphere respirator  
36  
37 642 (1860). \*Horizontal solid line represents the N95 filtration efficiency requirement of  $\geq 95\%$   
38  
39  
40 643 particle filtration efficiency according to 42 CFR Part 84. \*\*Horizontal lines represent the  
41  
42 644 following breathing resistance standards: Inhalation:  $\leq 35$  mmH<sub>2</sub>O; exhalation:  $\leq 25$  mmH<sub>2</sub>O for  
43  
44  
45 645 respirators according to 42 CFR Part 84. Note: EN 149 maximum inhalation resistance at 95  
46  
47 646 L/min is 2.4 mbar, or approximately 24 mmH<sub>2</sub>O. At higher flow rate according to EN 149, the  
48  
49  
50 647 equivalent breathing resistance may increase slightly but can be similar to the 42 CFR Part 84  
51  
52 648 maximum inhalation resistance at 85 L/min.

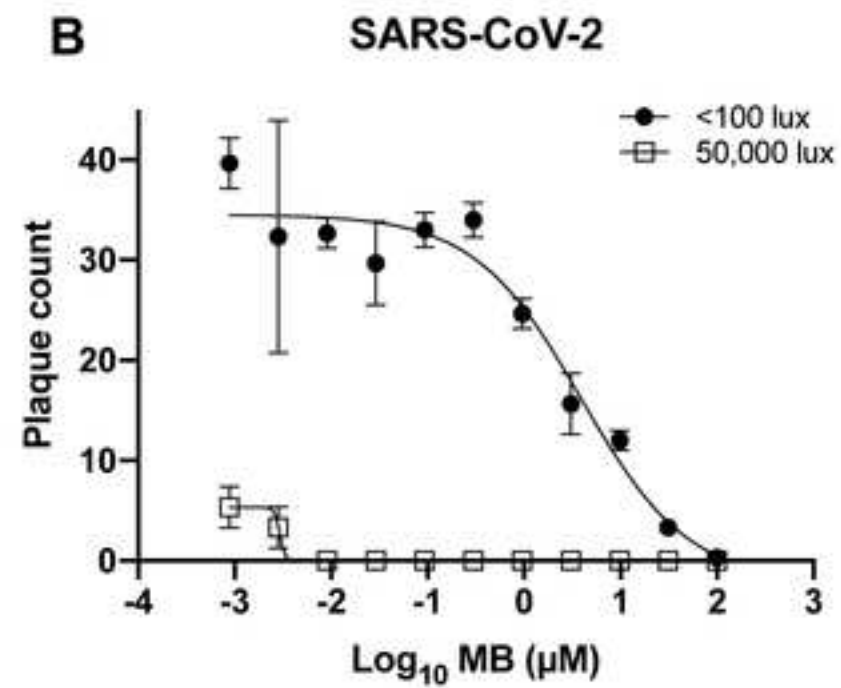
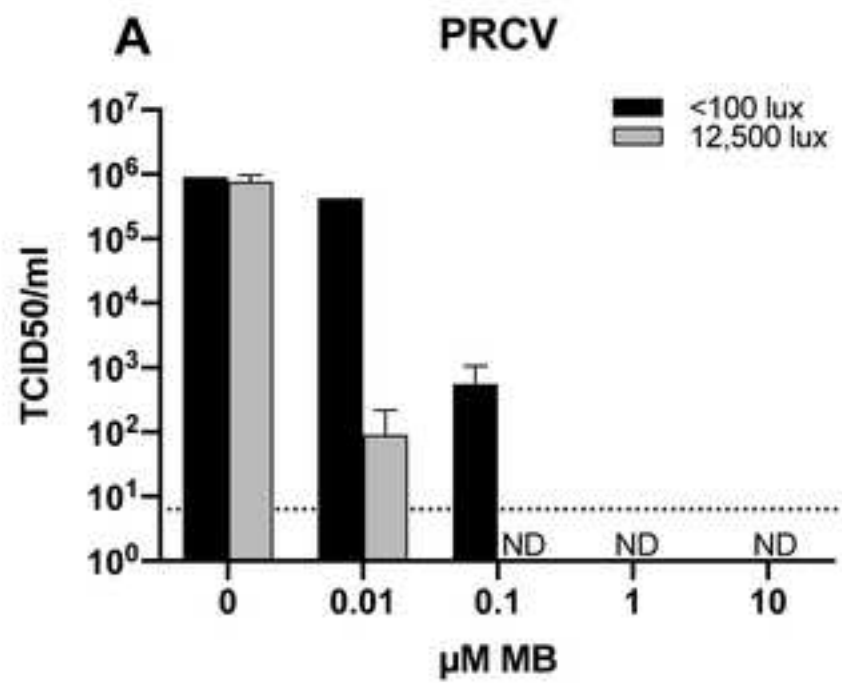
53  
54  
55 649 RH= Halyard duckbill respirator (Fluidshield-46727). RM= 3M half-sphere respirator (1860).  
56  
57 650 R3= 3M panel respirator (1870+). FW= EN 14683 Type II generic face mask. FH= ASTM  
58  
59 651 F2100 Level 2 Halyard face mask.  
60  
61  
62  
63  
64  
65

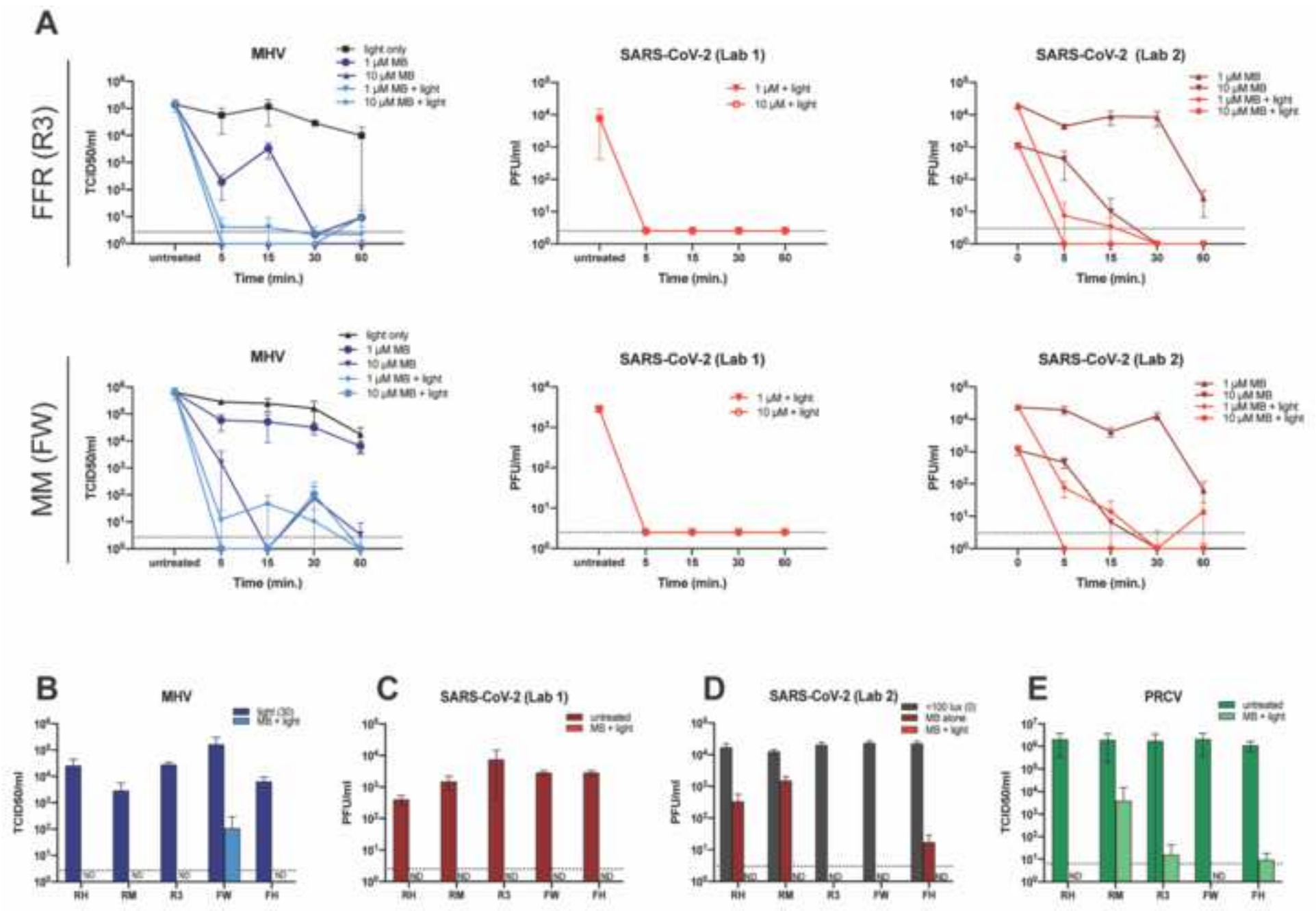
1  
2  
3  
4 652 **FIGURE 6. Effect of MBL and VHP+O<sub>3</sub> treatments on human and manikin fit factor of**  
5  
6 653 **FFR/MMs. (A) We performed human fit testing with volunteer participants who adjusted the**  
7  
8 654 **FFR and MM to achieve the highest fit factor or seal and subsequently performed head**  
9  
10 655 **movements and remeasured fit or seal. (B) Manikin fit factors using advanced, realistic manikin**  
11  
12 656 **headforms is a reproducible method to test fit without volunteer participants. We used the**  
13  
14 657 **PortaCount® PRO+ 8038 machine to determine overall fit for both human participants and**  
15  
16 658 **manikins headforms. \*Indicates significantly different values between treated and untreated FFR**  
17  
18 659 **or MM at p<0.05, Student's t- test or Mann-Whitney U test, as appropriate. \*\*Horizontal line**  
19  
20 660 **represents the following standard: ≥100; OSHA 29 CFR 1910.134(f)(7). Percentages on or**  
21  
22 661 **above each bar represents % of respirators or masks tested that surpassed this standard. While**  
23  
24 662 **the standard does not apply to face masks, we present the % to note the strong difference**  
25  
26 663 **between respirator and face mask test results. †Horizontal solid line represents the following**  
27  
28 664 **standard: Per OSHA 1910.134(f)(7), if the Overall Fit Factor as determined through an OSHA-**  
29  
30 665 **accepted quantitative fit testing protocol is equal to or greater than 100 for tight-fitting half**  
31  
32 666 **facepieces, then the fit test has been passed for that respirator. RH=Halyard duckbill respirator**  
33  
34 667 **(Fluidshield-46727). RM=3M half-sphere respirator (1860). R3=3M panel respirator (1870+).**  
35  
36 668 **FW=EN 14683 Type II generic face mask. FH=ASTM F2100 Level 2 Halyard face mask.**  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60  
61  
62  
63  
64  
65

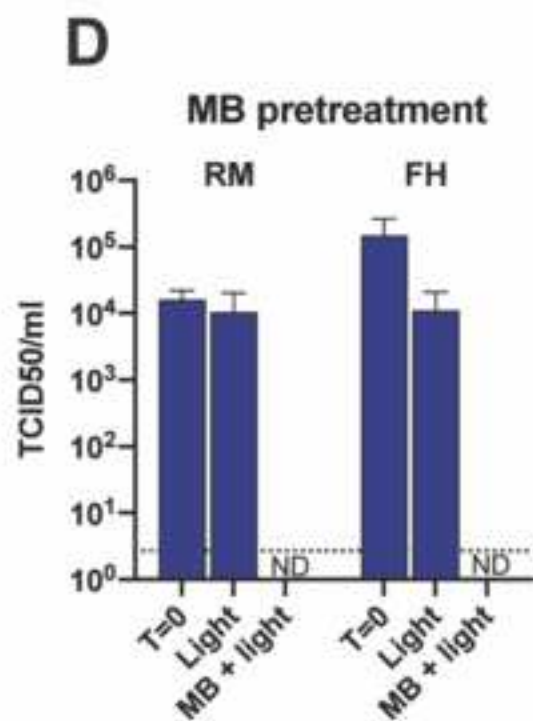
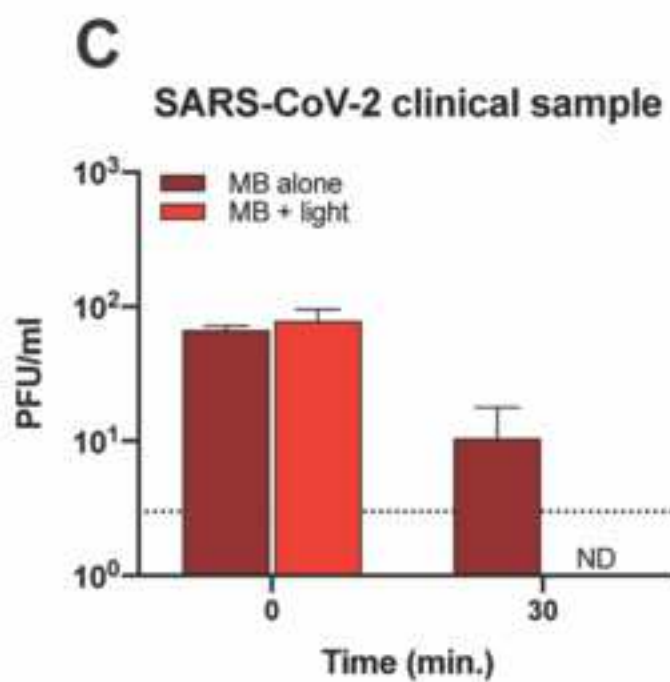
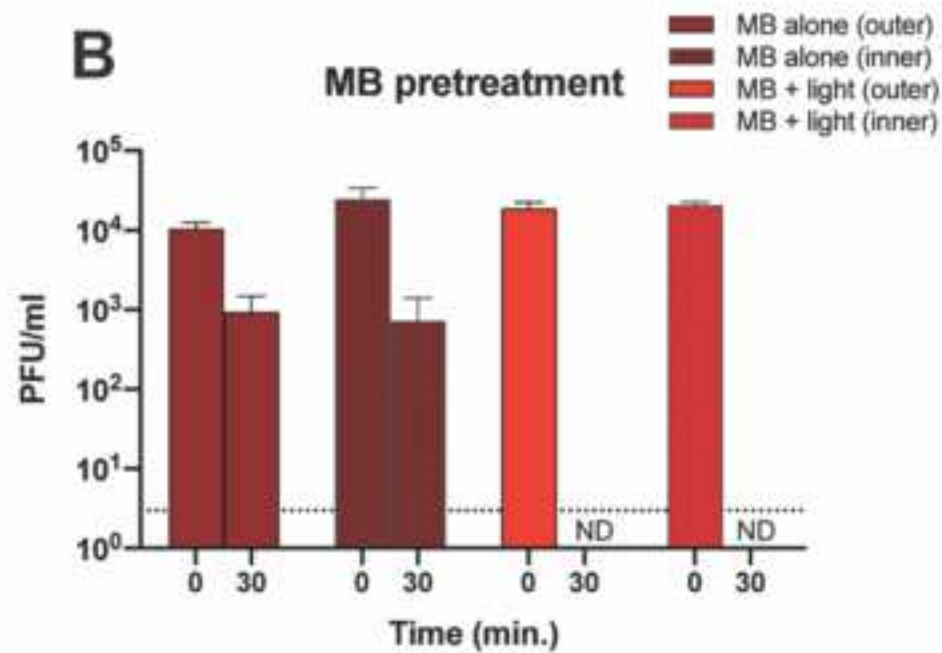
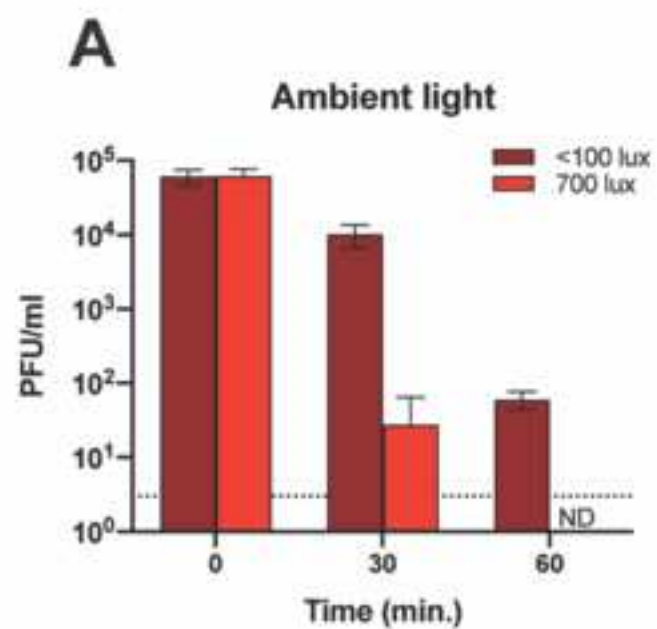
**DeMaND Graphical Abstract** – Decontamination of masks and filtering facepiece respirators using methylene blue photochemical treatment

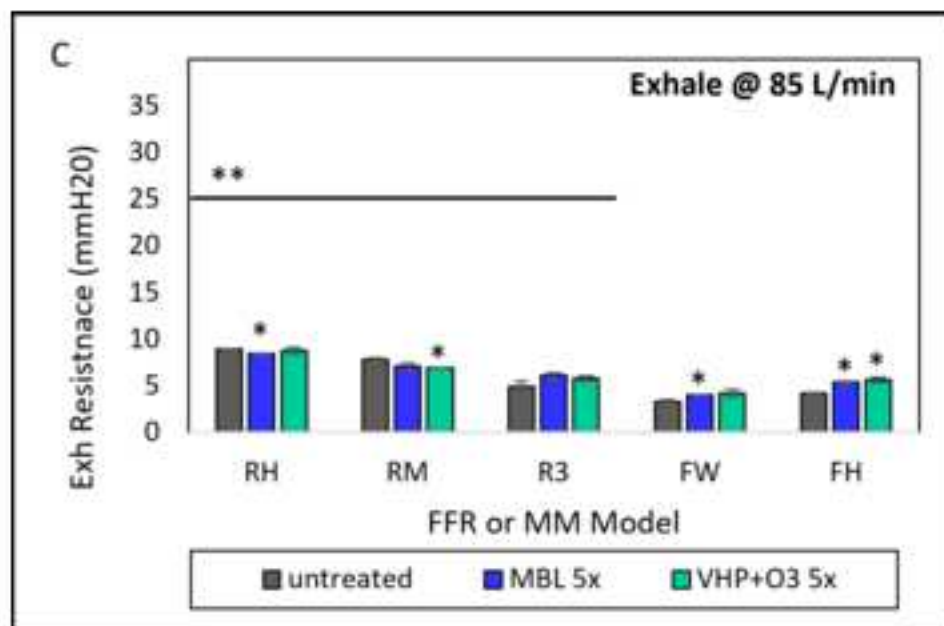
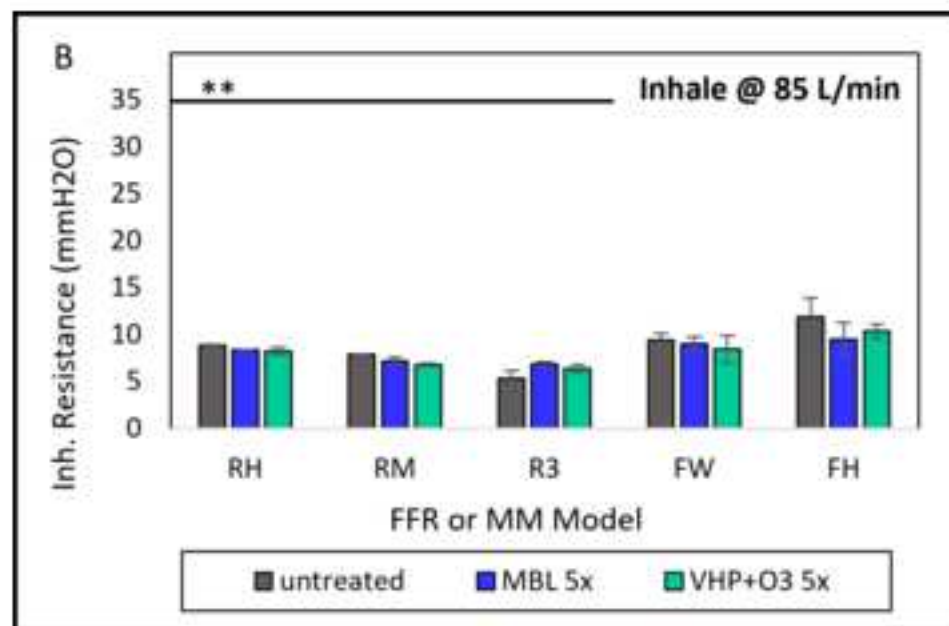
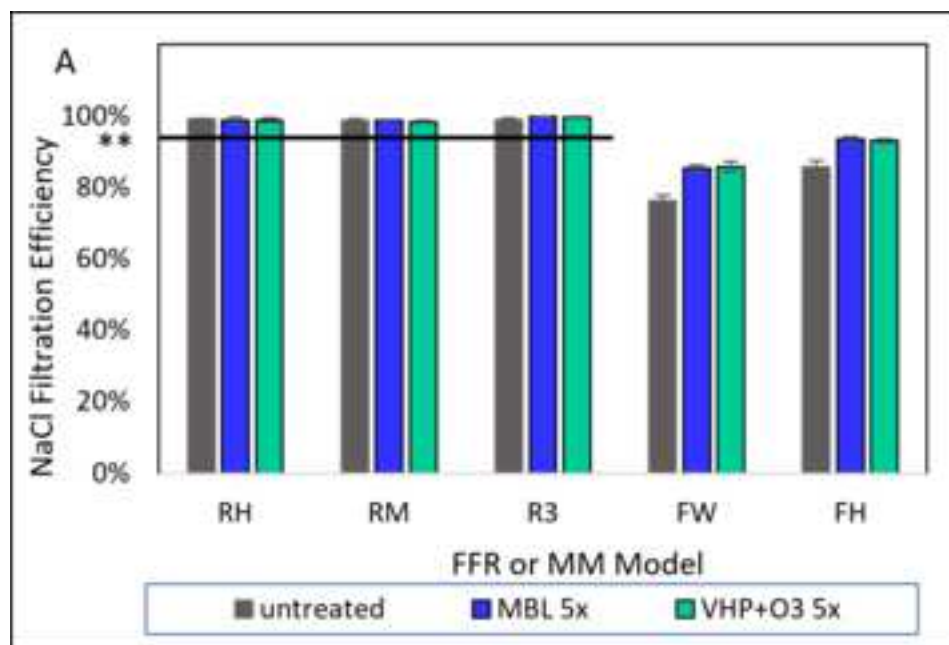


Panel A: Viruses, decontamination methods and personal protective equipment used in the DeMaND study. Panel B: Virus inactivation testing process. Panel C: Integrity testing process. Abbreviations: PRCV = porcine respiratory coronavirus, SARS-CoV-2 = severe acute respiratory syndrome coronavirus 2, MHV = murine hepatitis virus, MBL = methylene blue + light, VHP+O<sub>3</sub> = vaporized hydrogen peroxide plus ozone

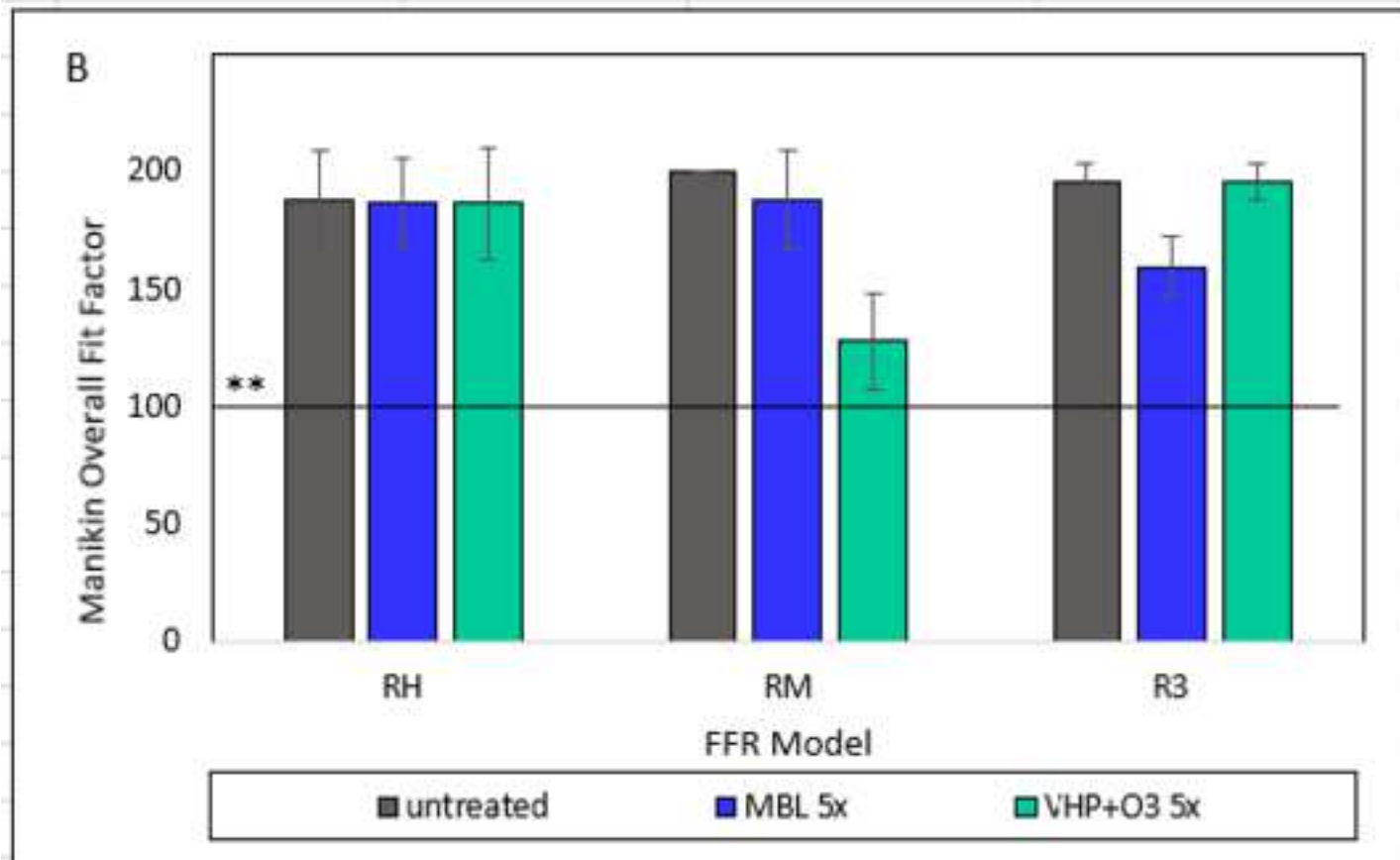
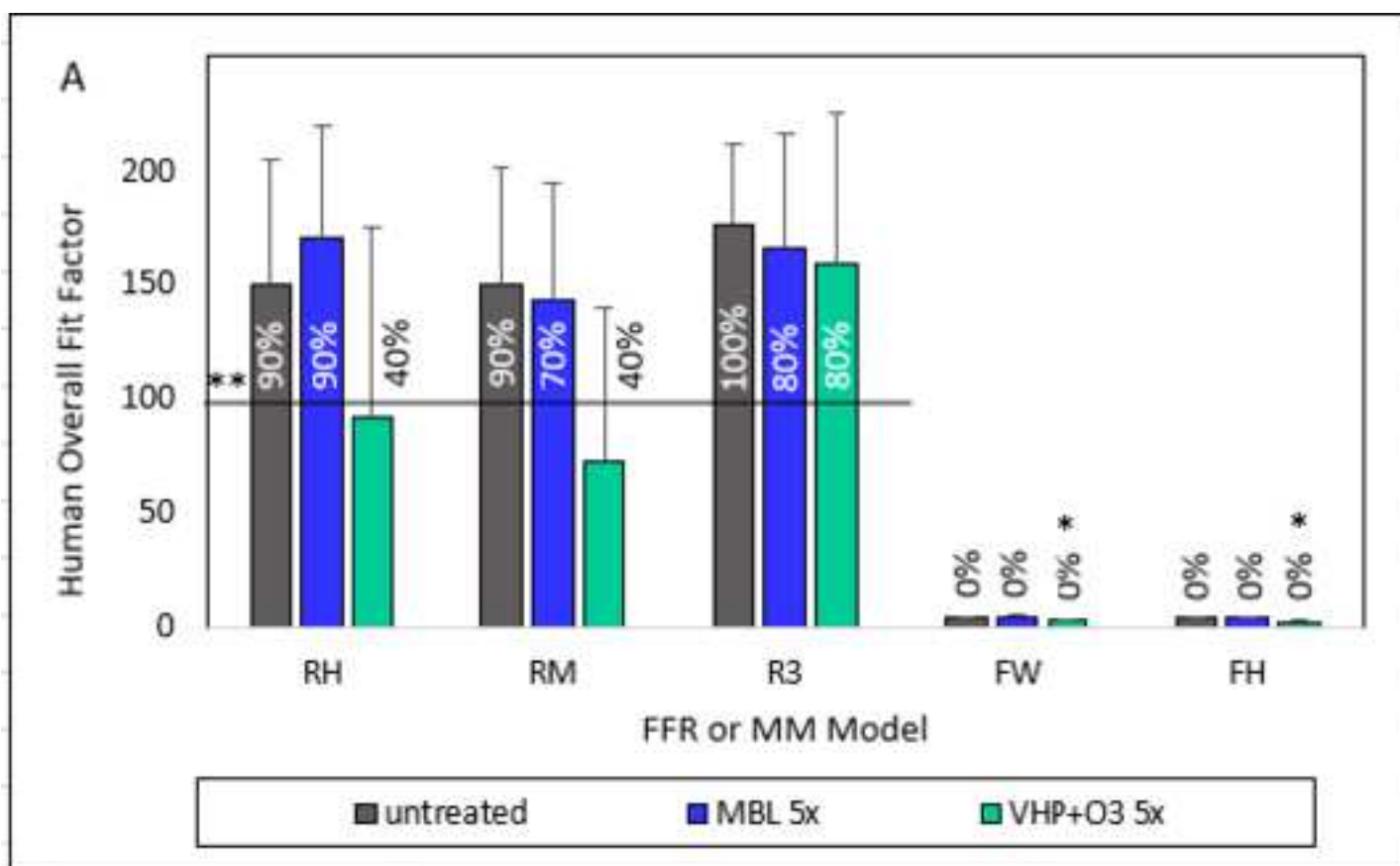








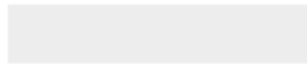






[Click here to access/download](#)


**Supplementary Material (for online publishing only)**  
Lendvay\_Supplemental Table S1\_Mar\_1\_2021.docx





[Click here to access/download](#)

**Supplementary Material (for online publishing only)**  
**Lendvay\_Supplemental Table S2A-B\_Mar\_1\_2021.docx**





[Click here to access/download](#)

**Supplementary Material (for online publishing only)**

**Lendvay\_SUPPLEMENT\_Mar\_1\_2021.docx**

